Estimation of stochastic behaviour in cardiac myocytes: I. Calcium movements inside the cytosol and sarcoplasmic reticulum on curvilinear domains

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Abstract

**Background:** Since the discovery of Ca$^{2+}$ sparks and their stochastic behaviour in cardiac myocytes, models have focused on the inclusion of stochasticity in their studies. While most models pay more attention to the stochastic modelling of cytosolic Ca$^{2+}$ concentration the coupling of Ca$^{2+}$ sparks and blinks in a stochastic model has not been explored fully. The cell morphology in past in silico studies is assumed to be Cartesian, spherical or cylindrical. The application on curvilinear grids can easily address this restriction and provide more realistic cell morphology. This paper presents a stochastic reaction-diffusion model that couples Ca$^{2+}$ sparks and blinks applied to curvilinear domains.

**Methodology:** Transformation of the model was performed to the curvilinear coordinate system. A set of differential equations is used to produce Ca$^{2+}$ waves initiated from sparks and blinks. A non-buffered and non-dyed version as well as a buffered and dyed version of these equations were studied in light of observing the effects of reactions on the Ca$^{2+}$ wave properties. For comparison, results for both the Cartesian and curvilinear grids are provided.

**Results and Conclusions:** A successful demonstration of the application of curvilinear grids serving as basis for future developments.

**Keywords**
Stochastic calcium waves, Ca$^{2+}$ sparks and blinks, curvilinear domain.

Introduction

Ca$^{2+}$-induced Ca$^{2+}$ release (CICR) is the repeated process in which influx of extracellular Ca$^{2+}$ into the cytosol from L-type channels triggers a release of Ca$^{2+}$ from the sarcoplasmic reticulum (SR) through ryanodine receptors (RyRs) on the z-lines [1]. The CICR process is schematically illustrated in Figure 1 (a more detailed review of the processes leading to contraction can be found here [2]). The calcium release event appears as Ca$^{2+}$ sparks [3, 4, 5, 6, 7, 8] in the cytosol and Ca$^{2+}$ blinks [9] in the SR. The successive activation of RyRs increases the local Ca$^{2+}$ concentration in the cytosol. This process is called calcium transient [10, 11, 12].
It is of particular importance to understand the underlying mechanism of the CICR process since in cardiac ventricle cells spontaneous propagating waves of Ca$^{2+}$ may occur due to Ca$^{2+}$ overload which is believed to occur under pathological conditions. This can affect the heart’s normal function and may lead to ventricular arrhythmias and heart failure [13, 14].

Ca$^{2+}$ sparks in the heart muscle were first recorded by Cheng et al. (1993) [3]. Using confocal imaging and fluorescent indicator fluo-3, they observed discrete regions of increased fluorescence that varied in position between sequences of images that were taken 0.5 seconds apart. These increases correspond to spontaneous increases in intracellular Ca$^{2+}$, [Ca$^{2+}$], known as Ca$^{2+}$ sparks. The increases appear to originate from point sources of Ca$^{2+}$ since they are restricted to circular regions. To investigate the origins of these sparks, cells were exposed to bathing medium without Ca$^{2+}$ as to block entry of extracellular Ca$^{2+}$ through sarcolemmal channels. This allowed them to investigate the role of SR Ca$^{2+}$ release. Under normal physiological conditions it was found that the opening rate of the RyR was low and propagating CICR does not occur. The observed propagating waves of CICR was suggested to be due to the increased sensitivity of the CICR to the increase in [Ca$^{2+}$].

Spatial non-uniformity was observed with the Ca$^{2+}$ release [4] and it was found that these releases occur at discrete sites closely associated with transverse (t)-tubules at Z-lines [15] with regular spacing of 1.8-1.9µm longitudinally and more irregularly with a mean value of 0.79µm transversely [8]. There is no systematic spatial pattern in the spark occurrence and the occurrence varies temporally as well as spatially, therefore, exhibiting stochastic behaviour [4]. A study undertaken by Cannell et al. (1995) reported that the probability density function of the spark

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**Figure 1.** Schematic view of the influx and efflux of calcium in a cardiac myocyte. Ca$^{2+}$ entry through L-type channels on the sarcolemma triggers Ca$^{2+}$ release from the SR. This is a repeated process of the CICR mechanism. The calcium released from the SR increases the concentration in the cytosol. Ca$^{2+}$ here travels to the sarcomeres and interacts with filaments and activates the contractile machinery. Upon relaxation, Ca$^{2+}$ disassociates from the filaments and is pumped back into the SR by the SERCA pumps. Modified from [2].
occurrence fits a Poisson distribution, thus, supporting the idea that Ca\(^{2+}\) channel openings is a stochastic process [4].

Several models have been used to simulate the Ca\(^{2+}\) sparks and waves. A number of these models are partially based on the CICR process and the release from RyRs are described as either deterministic or stochastic. A non-exhaustive list of these models with a short description is given in Table 1 under two categories: deterministic and stochastic models. The models presented in Table 1 mainly consist of fractional differential equations (FDEs), partial differential equations (PDEs), and ordinary differential equations (ODEs).

Backx et al. (1989) described the CICR process with Magnesium buffer reactions using a one-dimensional model that only takes into account longitudinal diffusion [16]. The Ca\(^{2+}\) release from the SR occurs at calcium release units (CRUs) and is assumed to be a time dependent process with an exponential rise and fall of the Ca\(^{2+}\) flux from the SR. The occurrence was dependent on a threshold for Ca\(^{2+}\) concentration which lead to a deterministic description of this term in the model. A similar deterministic formulation was incorporated in the release flux by Soeller and Cannell (2002) which was then included in the total calcium current by volume integration [17]. The aim was to experimentally test the extraction of the release flux underlying calcium sparks including a more detailed dye and buffer binding structure.

**Table 1.** A non-exhaustive list of previously studied deterministic and stochastic models for the Ca\(^{2+}\) sparks and waves.

<table>
<thead>
<tr>
<th>Deterministic</th>
<th>FDE/PDE/ODE</th>
<th>Buffers and dye?</th>
<th>Citations</th>
</tr>
</thead>
<tbody>
<tr>
<td>Backx et al. 1989</td>
<td>PDE, 6 ODEs</td>
<td>Yes</td>
<td>[16]</td>
</tr>
<tr>
<td>Goldbeter et al. 1990</td>
<td>2 ODEs</td>
<td>No</td>
<td>[18]</td>
</tr>
<tr>
<td>Dupont &amp; Goldbeter, 1994; 1997</td>
<td>PDE, ODE</td>
<td>No</td>
<td>[19, 20]</td>
</tr>
<tr>
<td>Smith et al. 1998</td>
<td>2 PDEs, 4 ODEs</td>
<td>Yes</td>
<td>[21]</td>
</tr>
<tr>
<td>Izu et al. 1998, 2001a</td>
<td>2 PDEs, 2 ODEs</td>
<td>Yes</td>
<td>[22, 23]</td>
</tr>
<tr>
<td>Soeller &amp; Cannell, 2002</td>
<td>4 PDEs, 3 ODEs</td>
<td>Yes</td>
<td>[17]</td>
</tr>
<tr>
<td>Tan et al. 2007</td>
<td>FDE, PDE, ODE</td>
<td>Yes</td>
<td>[24]</td>
</tr>
<tr>
<td>Tracqui and Ohayon, 2009</td>
<td>PDE, ODE</td>
<td>No</td>
<td>[25]</td>
</tr>
<tr>
<td>Li et al. 2011</td>
<td>2 FDEs, 4 ODEs</td>
<td>Yes</td>
<td>[26]</td>
</tr>
</tbody>
</table>

<table>
<thead>
<tr>
<th>Stochastic</th>
<th>FDE/PDE/ODE</th>
<th>Buffers and dye?</th>
<th>Citations</th>
</tr>
</thead>
<tbody>
<tr>
<td>Izu et al. 2001b</td>
<td>2 PDEs, 2 ODEs</td>
<td>Yes</td>
<td>[27]</td>
</tr>
<tr>
<td>Lu et al. 2010</td>
<td>2 PDEs, 2 ODEs</td>
<td>Yes</td>
<td>[14]</td>
</tr>
<tr>
<td>Chen et al. 2013, 2014</td>
<td>FDE, PDE, 4 ODEs</td>
<td>Yes</td>
<td>[28, 29]</td>
</tr>
<tr>
<td>Li et al. 2017</td>
<td>FDE, 3 PDEs, 5 ODEs</td>
<td>Yes</td>
<td>[30]</td>
</tr>
</tbody>
</table>

Another deterministic construction of the SR calcium release was represented in 2 dimensional models [22, 23, 21] so the spatial and anisotropic properties of the cytosolic Ca\(^{2+}\) diffusion can
be successfully reproduced. In these models, the diffusion of Ca$^{2+}$ sparks obeys Fick’s Law. Later on, an anomalous subdiffusion model was proposed based on a FDE that represents the cytosolic Ca$^{2+}$ concentration [24, 26] and it was shown to reproduce the spatial characteristic of sparks more realistically.

There has also been deterministic models with no buffer reactions included [18, 19, 20]. These models focused on representing the CICR process in a compartmental model with no dye and buffer reactions. No virtual point sources of CRUs are described. Instead the SR Ca$^{2+}$ release is associated with a nonlinear term based on the cytosolic and sarcoplasmic concentrations applied to all spatial points of the computational domain. In 2009, this two-pool CICR model was integrated into a force-calcium relation by Tracqui and Ohayon to successfully reproduce Ca$^{2+}$ waves and the resulting phases of contraction using cylindrical coordinates [25].

More recently, stochasticity is introduced into models [27] in which the Ca$^{2+}$ channel opening depends on a probability function. The distribution of the CRUs were made discrete with longitudinal distancing of 2μm and transverse distancing of 0.4-0.8μm. Lu et al. (2010) integrated rogue RyRs into this model to simulate the effect of these receptors on the Ca$^{2+}$ wave in ventricular myocytes with heart failure [14]. These models were extended from Fick’s Law based Ca$^{2+}$ diffusion to anomalous subdiffusion [28, 29]. Except for the work by Li et al. (2017) [30] the coupling of Ca$^{2+}$ concentration in the cytosol to that in the SR has not been performed. Additionally, to this date models have been implemented on Cartesian, spherical [17] and cylindrical coordinates [31] which is a simplification towards representing the actual cell morphology. No stochastic or deterministic model are represented on curvilinear domains.

The aim of the present paper is the 1) extension of the stochastic formulation by Izu et al. (2001b) [27] to include the Ca$^{2+}$ sparks coupled with Ca$^{2+}$ blinks and its application on curvilinear domains (this allows one to work on real cell morphology); 2) representation of two different systems: a) buffered and dyed system to account for calcium movement observed in in vitro studies and b) non-buffered and non-dyed system to be able to distinguish the effects that reactions have on the dynamics; 3) comparison of the Cartesian and curvilinear domains. The model and its extension to curvilinear grids are described in the next section. The application to curvilinear grids and comparison results between models are presented in the results section with conclusions and potential future improvements discussed in the final section of this paper.

**Methods**

*Mathematical model for Ca$^{2+}$ sparks and Ca$^{2+}$ blinks with buffer and dye*

The set of differential equations (DEs) by Izu et al. (1998, 2001a, 2001b) [22, 23, 27] describing the cytosolic Ca$^{2+}$ concentration with buffer and dye binding properties is modified to include an additional term for the cytosolic leak from [19, 20, 25] and a slightly different representation of the SR leak term [19, 20, 25]. An extension to this model here includes a coupling of the cytosolic Ca$^{2+}$ diffusion with the sarcoplasmic Ca$^{2+}$ concentration. For simplicity, diffusion is restricted to follow Fick’s Law. Considering the above, the reaction-diffusion equations are expressed as

$$
\frac{\partial C_{\text{cyt}}}{\partial t} = D_{Cx} \frac{\partial^2 C_{\text{cyt}}}{\partial x^2} + D_{Cy} \frac{\partial^2 C_{\text{cyt}}}{\partial y^2} + J_{\text{dye}} + J_{\text{buffer}} - J_{\text{pump}} - J_{\text{Ca}^{2+}\text{leak}} + J_{\text{CRU}} - J_{\text{SR leak}}
$$

(1)
\[
\frac{\partial C_{SR}}{\partial t} = J_{SR\,\text{leak}} + J_{\text{pump}} - J_{\text{CRU}} + J_{\text{dye}} + J_{\text{buffer}} \tag{2}
\]
\[
\frac{\partial [CaF]}{\partial t} = D_{Dx} \frac{\partial^2 [CaF]}{\partial x^2} + D_{Dy} \frac{\partial^2 [CaF]}{\partial y^2} - J_{\text{dye}} \tag{3}
\]
\[
\frac{\partial [CaB]}{\partial t} = -J_{\text{buffer}} \tag{4}
\]

where \(C_{\text{cyt}} = [Ca^{2+}]_{\text{cyt}}\) is the free \(Ca^{2+}\) concentration in the cytosol; \(C_{SR} = [Ca^{2+}]_{SR}\) is the free \(Ca^{2+}\) concentration in the SR; \([CaF]\) and \([CaB]\) are the concentrations of \(Ca^{2+}\) bound dye and buffer; \(D_{Cx}\) and \(D_{Cy}\) are cytosolic \(Ca^{2+}\) diffusion coefficients in the longitudinal and transverse directions; \(D_{Dx}\) and \(D_{Dy}\) are diffusion coefficients of the \(Ca^{2+}\) bound dye in the longitudinal and transverse directions, respectively. \(Ca^{2+}\) diffusion is reported to be anisotropic [32] with diffusion twice as fast along the sarcomere orientation than that in the transverse direction [31]. Standard values used satisfy experimental data that \(\frac{D_{Cy}}{D_{Cx}} = 0.5\) and are given in Table 2 along with a short description. Fluxes due to \(Ca^{2+}\) fluorescent indicator dye, \(J_{\text{dye}}\), and endogenous stationary buffers, \(J_{\text{buffer}}\), are

\[
J_{\text{dye}} = -k_{F}^{+}C_{\text{cyt}}([F]_{T} - [CaF]) + k_{F}^{-}[CaF]
\]
\[
J_{\text{buffer}} = -k_{B}^{+}C_{\text{cyt}}([B]_{T} - [CaB]) + k_{B}^{-}[CaB]
\]

\(k_{F}^{+}\) and \(k_{F}^{-}\) are forward and reverse rate constants for dye (\(j = F\)) and buffer (\(j = B\)); \([F]_{T}\) and \([B]_{T}\) are total concentration of the indicator dye and buffers, values of which are given in Table 2. \(J_{\text{pump}}, J_{\text{Ca}^{2+}\,\text{leak}}, J_{\text{SR\,leak}}\) represent the pumping rate of SR \(Ca^{2+}\)-ATPase, \(Ca^{2+}\) leak from the cytosol and SR, respectively. These are given as

\[
J_{\text{pump}} = V_{\text{pump}} \frac{n_{\text{pump}}^{\text{pump}} C_{\text{cyt}}}{K_{\text{pump}}^{\text{pump}} + C_{\text{cyt}}^{n_{\text{pump}}}^{\text{pump}}}
\]
\[
J_{\text{Ca}^{2+}\,\text{leak}} = kC_{\text{cyt}}
\]
\[
J_{SR\,\text{leak}} = k_{f}C_{SR}
\]

in which \(V_{\text{pump}}, K_{\text{pump}}\) and \(n_{\text{pump}}\) represent the maximal rate, affinity constant and the Hill exponent for \(Ca^{2+}\) uptake into SR, while \(k\) and \(k_{f}\) are constants for \(Ca^{2+}\) efflux from cytosol to extracellular medium and from SR into cytosol, respectively.

**Table 2.** Standard parameter values [22, 23, 27, 28, 29].

<table>
<thead>
<tr>
<th>Parameter</th>
<th>Value</th>
<th>Units</th>
<th>Notes</th>
</tr>
</thead>
<tbody>
<tr>
<td>(D_{Cx}, D_{Cy})</td>
<td>0.3, 0.15</td>
<td>(\mu m^2/\text{ms})</td>
<td>(Ca^{2+}) diffusion coefficients</td>
</tr>
<tr>
<td>(D_{Dx}, D_{Dy})</td>
<td>0.02, 0.01</td>
<td>(\mu m^2/\text{ms})</td>
<td>Diffusion coefficients of dye</td>
</tr>
<tr>
<td>(l_x, l_y)</td>
<td>2, 0.8</td>
<td>(\mu m)</td>
<td>Spacing of CRUs in x and y</td>
</tr>
<tr>
<td>([Ca^{2+}]_{\text{cyt}}(\infty))</td>
<td>0.1</td>
<td>(\mu M)</td>
<td>Initial (Ca^{2+}) concentration</td>
</tr>
<tr>
<td>(F)</td>
<td>96500</td>
<td>(C,\text{mol}^{-1})</td>
<td>Faraday’s constant</td>
</tr>
<tr>
<td>(V_{\text{pump}})</td>
<td>0.208</td>
<td>(\mu M/\text{ms})</td>
<td>Maximum SR pump rate</td>
</tr>
<tr>
<td>Parameter</td>
<td>Value</td>
<td>Description</td>
<td></td>
</tr>
<tr>
<td>--------------------</td>
<td>------------------</td>
<td>--------------------------------------------------</td>
<td></td>
</tr>
<tr>
<td>$K_{pump}$</td>
<td>0.184 $\mu$M</td>
<td>SR pump Michaelis constant</td>
<td></td>
</tr>
<tr>
<td>$K_{prob}$</td>
<td>15 $\mu$M</td>
<td>Ca$^{2+}$ sensitivity parameter</td>
<td></td>
</tr>
<tr>
<td>$n_{pump}$, $n_{prob}$</td>
<td>3.9, 1.6</td>
<td>Hill coefficients</td>
<td></td>
</tr>
<tr>
<td>$T_{open}$</td>
<td>10 ms</td>
<td>Duration of current flow through CRU</td>
<td></td>
</tr>
<tr>
<td>$P_{max}$</td>
<td>0.3 per CRU ms$^{-1}$</td>
<td>Maximum probability of Ca$^{2+}$ spark occurrence</td>
<td></td>
</tr>
<tr>
<td>$\sigma_3$</td>
<td>$I_{CRU}/2F$ mole/ms</td>
<td>3 dimensional Ca$^{2+}$ source strength</td>
<td></td>
</tr>
<tr>
<td>$k_f^+, k_B^+$</td>
<td>80, 100 $(\mu$Ms$)^{-1}$</td>
<td>Forward rate constants for dye and buffer reactions</td>
<td></td>
</tr>
<tr>
<td>$k_f^-, k_B^-$</td>
<td>90, 100 s$^{-1}$</td>
<td>Reverse rate constants for dye and buffer reactions</td>
<td></td>
</tr>
<tr>
<td>$[F]_T, [B]_T$</td>
<td>50, 123 $\mu$M</td>
<td>Total concentration (bound + unbound) of fluorescent dye and buffer</td>
<td></td>
</tr>
</tbody>
</table>

The SR Ca$^{2+}$ release term, $J_{CRU}$, is expressed as [14, 27, 28, 29]

$$J_{CRU} = \sigma \sum_{i,j} \delta(x - x_i)\delta(y - y_j)S(x_i, y_j; T_{open}), \quad \sigma = K_s \sigma_3$$

Molar flux through the RyRs, $\sigma$, is associated with the source strength, $K_s$, and the 3 dimensional source strength, $\sigma_3 = I_{CRU}/2F$. $K_s$ needs to be derived for a 2 dimensional model (See equation A1 in Appendix).

The CRUs are placed at regular intervals of $l_x$ along the x-axis and $l_y$ along the y-axis. It is assumed that once a CRU opens it will remain open for 10ms (i.e. $T_{open} = 10$) after which it will switch to a closed state and will not reopen (a long refractory period). An adjustment to the source strength was previously done to approximate the molar flux of a point source [23]. This approach is adopted here for a general 2 dimensional case [33] (See Appendix for the obtained $\sigma$ values for the 2 dimensional case). The locations of the CRUs are identified through the Dirac delta function, $\delta$ where there is a channel (i.e. $x - x_i = 0$ implies that $\delta = 1$ which denotes there is a channel otherwise $x - x_i \neq 0$ indicates no channel $\delta = 0$). The stochastic term, $S$, controls the firing of the CRU when a probability condition is satisfied

$$S(x_i, y_j; T_{open}) = \begin{cases} 1, & P/P_{max} > u \\ 0, & P/P_{max} \leq u \end{cases}$$

where $P(C(x,y,t), K_{prob}, n_{prob}) = P_{max}C_{cyt}^{n_{prob}}/(K_{prob}^{n_{prob}} + C_{cyt}^{n_{prob}})$, $P_{max}$ is the maximum probability of Ca$^{2+}$ spark occurrence, $K_{prob}$ represents the Ca$^{2+}$ sensitivity factor and $n_{prob}$ is the Hill coefficient. At each time step, $\Delta t$, a uniformly distributed random number, $u$, is generated and compared to the probability function $P$ calculated from the Ca$^{2+}$ concentration. A CRU fires if $P/P_{max} > u$ and thus $S = 1$ otherwise (i.e. in the case where $P/P_{max} < u$) a CRU will remain closed, i.e. $S = 0$.

**Cartesian and curvilinear domains**

Two different systems were solved on the Cartesian and curvilinear domains: 1) non-buffered and non-dyed (NBND) system (i.e. $J_{dye} = J_{buffer} = 0$) and; 2) buffered and dyed (BD) system.
Certain parameter values such as the initial SR Ca\(^{2+}\) concentration (i.e. \([Ca^{2+}]_{SR(\infty)}\)), \(k\), \(k_f\), and \(I_{CRU}\) required modification when moving from a NBND system to a BD system in order to achieve a strong propagation of Ca\(^{2+}\) wave. These parameter values are given in Table 3.

### Table 3. Parameter values for NBND and BD cases applied to the Cartesian and curvilinear grids. Some values used in the case of the BD system are within the range of the cited values.

<table>
<thead>
<tr>
<th>Parameter</th>
<th>NBND</th>
<th>BD</th>
</tr>
</thead>
<tbody>
<tr>
<td>([Ca^{2+}]_{SR(\infty)})</td>
<td>750</td>
<td>1000</td>
</tr>
<tr>
<td>(k)</td>
<td>2</td>
<td>[25]</td>
</tr>
<tr>
<td>(k_f)</td>
<td>0.2</td>
<td>[25]</td>
</tr>
<tr>
<td>(I_{CRU})</td>
<td>6</td>
<td>30</td>
</tr>
</tbody>
</table>

A 2 dimensional domain is considered with the Cartesian and curvilinear grids shown in Figure 2. The Cartesian problem (Figure 2 - top) is solved with equations (1)–(4). Discretisation of the PDEs is performed using the alternating direction implicit (ADI) method. The ODE for the sarcoplasmic Ca\(^{2+}\) concentration is discretised using a 4\(^{th}\) order Adams-Bashforth (AB) method and the other ODEs are discretised using the traditional forward Euler method.

In the curvilinear case, the diffusive equations (1) and (3) need to be transformed from the Cartesian based system to the curvilinear coordinate system prior to discretising. Transforming equations (1) and (3) they become

\[
\frac{\partial [Ca^{2+}]_{cyt}}{\partial t} = \left( D_{Dx} \left( \frac{\partial [Ca^{2+}]_{cyt}}{\partial x} \right)^2 + D_{Dy} \left( \frac{\partial [Ca^{2+}]_{cyt}}{\partial y} \right)^2 \right) \frac{\partial^2 [Ca^{2+}]_{cyt}}{\partial \xi^2} + 2 \left( D_{Dx} \frac{\partial [Ca^{2+}]_{cyt}}{\partial x} \frac{\partial [Ca^{2+}]_{cyt}}{\partial y} \right) \frac{\partial^2 [Ca^{2+}]_{cyt}}{\partial \xi \partial \eta} + \left( D_{Dx} \left( \frac{\partial [Ca^{2+}]_{cyt}}{\partial x} \right)^2 + D_{Dy} \left( \frac{\partial [Ca^{2+}]_{cyt}}{\partial y} \right)^2 \right) \frac{\partial^2 [Ca^{2+}]_{cyt}}{\partial \eta^2} + \frac{J_{dye}}{\partial t} + J_{buffer} - J_{pump} - J_{Ca^{2+} leak} + J_{CRU} - J_{SR leak} \tag{5}
\]

\[
\frac{\partial [Ca^{2+}]_{F}}{\partial t} = \left( D_{Dx} \left( \frac{\partial [Ca^{2+}]_{F}}{\partial x} \right)^2 + D_{Dy} \left( \frac{\partial [Ca^{2+}]_{F}}{\partial y} \right)^2 \right) \frac{\partial^2 [Ca^{2+}]_{F}}{\partial \xi^2} + 2 \left( D_{Dx} \frac{\partial [Ca^{2+}]_{F}}{\partial x} \frac{\partial [Ca^{2+}]_{F}}{\partial y} \right) \frac{\partial^2 [Ca^{2+}]_{F}}{\partial \xi \partial \eta} + \left( D_{Dx} \left( \frac{\partial [Ca^{2+}]_{F}}{\partial x} \right)^2 + D_{Dy} \left( \frac{\partial [Ca^{2+}]_{F}}{\partial y} \right)^2 \right) \frac{\partial^2 [Ca^{2+}]_{F}}{\partial \eta^2} - J_{dye} \tag{6}
\]

These equations are then discretised using the ADI method. The source strength becomes spatially dependent since the distance between grid points will not be uniform. Equations (2), and (4)-(6) are then solved on the curvilinear grid (Figure 2 - bottom).
Orthogonal curvilinear coordinates are generated using the software gridgen-c developed by Sakov and CSIRO Marine Research (2000-2009) [See acknowledgement]. The code incorporates a CRDT algorithm by Driscoll and Vavasis (1998) for conformal mapping [34] which smoothly distributes the grid points throughout the domain.

The CRUs are distributed with \( l_x = 2 \mu m \) spacing in the longitudinal and \( l_y = 0.8 \mu m \) spacing in the transverse directions. In the curvilinear case, the number of spacing between CRUs is determined by setting equal number of grid points between channels leading to a pointwise evenly spread channels in both directions. The distribution of these channels are given on both Cartesian and curvilinear grids in Figure 3.
As boundary conditions zero-flux is assumed at the cell boundaries by imposing \( \frac{\partial C_{\text{cyt}}}{\partial x} = \frac{\partial C_{\text{cyt}}}{\partial y} = 0 \). Similar assumption is imposed on the equation for the Ca\(^{2+}\) bound dye, i.e. \( \frac{\partial [CaF]}{\partial x} = \frac{\partial [CaF]}{\partial y} = 0 \).

**Results**

In cardiac myocytes, Ca\(^{2+}\) waves propagate as sharp bands [35] with velocities and frequencies that are high enough to allow for the simultaneous propagation of distinct fronts in a given individual cell. The latter type of wave has been called type 1 for convenience [36].

In the following results, Ca\(^{2+}\) waves of type 1 is observed. Once sparks are initiated they develop in 10ms and increase the concentration around the region. The probability of firing is proportionally dependent on the local concentration. Therefore, a rise in concentration increases the probability of SR release and eventually leading to the activation of neighbouring CRUs. If the concentration is sufficiently high more CRUs fire consecutively which creates a propagating Ca\(^{2+}\) wave.

In all cases that are presented in this section, the initial cytosolic Ca\(^{2+}\) concentration at rest is set to \([Ca^{2+}]_{\text{cyt}(\infty)} = 0.1\mu M\). The concentration in the SR compartment is 500-1000 \(\mu M\) and is 2-3 orders of magnitude greater than that in the cytosol. Therefore, in the simulations presented here the initial concentration in the SR is set to 750 \(\mu M\) in the NBND system and 1000 \(\mu M\) in the BD systems. Simulations begin with 5x4 CRUs in the middle of the domain force activated in order to set off initial sparks. The temporal grids are set up with time step size of \(\Delta t = 0.1\). The spatial step sizes in the Cartesian case are set to \(\Delta x = \Delta y = 0.4\) and that in the curvilinear case is spatially dependent so will vary throughout the domain.

**NBND system on the Cartesian and curvilinear domains**

In this section, results are presented for the NBND system. The set of equations (1)-(4) are solved on the Cartesian domain and equations (2) and (4)-(6) on the curvilinear domain. Buffer and dye reactions are neglected in the model, i.e. \(J_{\text{dye}} = J_{\text{buffer}} = 0\), in order to observe the
effects of such reactions on the wave propagation velocity and amplitude. Solving the NBND system on both the Cartesian and curvilinear domains with the CRU distribution given in Figure 3, we obtain the results in Figures 4 (Cartesian) and 5 (curvilinear). Images show the development of the initial sparks in 10ms and its propagation towards and along the boundaries at the top and bottom until it reaches and propagates outwards from the boundaries at the ends (left and right).

Looking at the simulation time when the Ca$^{2+}$ reaches the end boundaries it was observed that the wave propagates in less time compared to that in the curvilinear case. As can be seen in Figure 6, the peak of the wave exits the domain in 200ms in the Cartesian (Figure 6 - a) and 400ms in the curvilinear (Figure 6 - b) cases. The longitudinal velocity of the wave is calculated to be approximately 289μm/s with amplitudes approximately ranging 17.1-19.3μM in the Cartesian (Figure 7 - a) and 153μm/s with amplitudes approximately ranging 19.2-23.3μM in the curvilinear cases (Figure 7 - c).

There is a periodic exchange of Ca$^{2+}$ between the SR and the cytosol. These result in the mentioned Ca$^{2+}$ sparks and blinks, the simulation results of which are presented in Figure 7. There is a slight difference in the amplitude of the cytosolic concentration profiles when comparing the Cartesian and curvilinear problems. Similarly, there is not much variation in the sarcoplasmic concentration profiles when comparing the solution on the two different domains.
In the Cartesian case, concentration in the SR drops to approximately $581\mu M$ while this drop in the curvilinear case is approximately between $576\mu M$ and $586\mu M$ (See Figure 7 – b and d).

**Figure 6.** Cytosolic $Ca^{2+}$ wave propagation without buffer and dye reactions. The spatial characteristics of the wave propagation are plotted on the (a) Cartesian domain at times 50, 100, 150 and 200 ms and (b) curvilinear domain at times 100, 200, 300 and 400ms.

**Figure 7.** Cytosolic (a and c) and sarcoplasmic (b and d) $Ca^{2+}$ concentrations are plotted on the Cartesian (a and b) and curvilinear (c and d) domains. Sensor 1 corresponds to a channel at the centre of the cell. Sensors 4 and 5 are $10\mu m$ away from sensor 1 on either side in the x-direction. Sensors 2 and 3 are quarter of the way in from the left and right edges, respectively.
**BD system on the Cartesian and curvilinear domains**

In this section, results are presented for the BD system. The same set of equations as in the previous section are solved but with reactions included, i.e. $I_{dye} \neq 0, I_{buffer} \neq 0$. Figures 8 and 9 show the Ca$^{2+}$ wave propagation in the presence of buffer and dye reactions. The wave velocity is observed to be approximately 113-114$\mu$m/s in the Cartesian and 111$\mu$m/s in the curvilinear coordinates. Figure 10 shows the time course of the Ca$^{2+}$ wave at times $t = 100, 200, 300$ and 400ms (a and c) and the normalised fluorescent indicator dye profile, $F/F_0$ (b and d). The normalised fluorescent indicator profile is recorded at the cell centre.

![Figure 8](image1.png)

**Figure 8.** Ca$^{2+}$ wave propagation on the Cartesian grid in the presence of buffer and dye reactions. Snapshots are recorded at times 10, 40, 75, 125, 175, 250, 350, 460 and 600 ms (left to right, top to bottom). The colourbar denotes the Ca$^{2+}$ concentration in $\mu$M.

![Figure 9](image2.png)

**Figure 9.** Ca$^{2+}$ wave propagation on the curvilinear grid in the presence of buffer and dye reactions. Snapshots are recorded at times 10, 40, 75, 150, 250, 350, 450, 600 and 900 ms (top to bottom left to right). The colourbar denotes the Ca$^{2+}$ concentration in $\mu$M.

The Ca$^{2+}$ concentration increases rapidly initially thus a steep rise in the normalised fluorescent value. The concentration is high enough so that neighbouring sites will activate eventually leading to wave of Ca$^{2+}$. As Ca$^{2+}$ propagates from the region the concentration will decrease leading to a decrease in the normalised fluorescent values. $F/F_0$ profile peaks at 1.129 and 1.135 in the Cartesian and curvilinear cases, respectively. The shape observed around the peak and the pattern of rise and fall is also observed in experimental [3-6, 8, 9, 17, 37- 39] and other numerical studies [17, 21, 24, 26].
A large variation is observed in the sparks and blinks (Figure 11). The amplitude of the sparks range 41.3-47.5μM with 81.7-85.2μM drop in SR Ca\(^{2+}\) content in the Cartesian case (Figure 11 - a) and that in the curvilinear case are 56.7-79μM for spark amplitude and 14.6-58.1μM for drop in SR Ca\(^{2+}\) concentration (Figure 11 - c).

**Figure 10.** Ca\(^{2+}\) wave propagation without buffer and dye reactions. The spatial characteristics of the wave propagation are plotted at times 100, 200, 300 and 400 ms on the (a) Cartesian and (c) curvilinear domains.
Discussion and conclusion

In this paper, the application of Ca\(^{2+}\) waves on the curvilinear grids is successfully demonstrated with comparisons against the Cartesian case. This enables the quantitative analysis on Ca\(^{2+}\) sparks/blinks and waves by taking into account more realistic cell morphology. The in silico study undertaken here included BD and NBND systems to distinguish the effects of reactions on the Ca\(^{2+}\) wave propagation on the Cartesian and curvilinear grids separately. It has been shown that in the case of the NBND system although not much variation was observed in the amplitudes of the cytosolic and sarcoplasmic Ca\(^{2+}\) concentration profiles, the wave velocity in the Cartesian case was much higher (almost twice as much) than that in the curvilinear case (which is closer to the experimentally observed value of 100\(\mu\)m/s). Adding buffer and dye to the system has dramatically changed the velocity and amplitude of the wave. Decrease in velocity was observed. The cytosolic Ca\(^{2+}\) amplitudes have increased by approximately 2.4 fold and SR Ca\(^{2+}\) content

**Figure 11.** Time course of the Ca\(^{2+}\) wave propagation located at sensors 1-5. Cytosolic Ca\(^{2+}\) concentrations are plotted on the (a) Cartesian and (c) curvilinear domains. Similarly, sarcoplasmic Ca\(^{2+}\) concentrations are plotted on the (b) Cartesian and (d) curvilinear domains. Sensor 1 corresponds to a channel at the centre of the cell. Sensors 4 and 5 are 10\(\mu\)m away from sensor 1 towards either side. Sensors 2 and 3 are quarter way in from the left and right edges, respectively.
drops to as much as approximately 6.85-7.1 fold in the Cartesian case whilst in the curvilinear case cytosolic Ca\(^{2+}\) have increased by roughly 3.5 times with a drop in SR Ca\(^{2+}\) content by 10-39 fold. In both the BD and NBND cases the wave velocity calculated on the curvilinear coordinate system provided a closer estimate to that observed experimentally (i.e. 100\(\mu\)m/s). In the BD cases, the fluorescent indicator dye profiles follow a pattern which is recorded experimentally.

The formation and development of Ca\(^{2+}\) sparks into waves appear differently in the Cartesian and curvilinear grids. The wave propagation region appears to be more elongated in the y-direction for the curvilinear cases. This may be due to either the distribution of CRUs being grid dependent or the partially contracted state of the cell morphology making the bottom half of the CRUs more dense and the top half coarser compared to the central part of the cell. The underlying algorithms used in the generation of curvilinear grid points ensure the orthogonal and conformal mapping of the grid points. Therefore, some regions will be densely or coarsely populated with grid points. Therefore, the distribution of CRUs will be dense or coarse in the respective regions accordingly. Having a spatially dependent distribution rather than a grid dependent one will make the curvilinear model more realistic since it is known that CRUs are longitudinally 2\(\mu\)m and transversely 0.4-0.8\(\mu\)m apart.

A single ODE was used as an update for a general buffer term. However, it is known that Ca\(^{2+}\) can bind to buffers consisting of calmodulin, troponin C, binding sites on the SR and sarcolemmal (SL) membranes. Therefore, a more detailed model must be incorporated to account for these buffers separately. Additionally, Ca\(^{2+}\) bound buffers and dye in the SR has different reaction and diffusional properties than that in the cytosol. Therefore, an additional set of equations accounting for this would make this model more comparable to the real case scenario. For the sarcoplasmic Ca\(^{2+}\) concentration, an ODE has been used. However, diffusion is also present in this compartment so a PDE can be used to account for this.

Recently, it has been shown that cytosolic Ca\(^{2+}\) diffusion follows an anomalous subdiffusion rather than Fick’s Law. Fick’s Law is known to produce Ca\(^{2+}\) full-width at half maximum (FWHM) of 1\(\mu\)m, half of which is observed experimentally. Anomalous subdiffusion is known to get around this issue and produce FWHM of closer to 2\(\mu\)m. Here transformation to curvilinear coordinates is more straightforward with Fick’s Law based diffusion. Bearing this in mind this simplification was maintained in order to demonstrate the application. The model presented in this paper can always be extended to an anomalous subdiffusion model.

**Appendix**

The numerical conversion for the source strength, \(K_s\), involves the Green’s function obtained from the analytical solution of the diffusion problem for the 2 dimensional case and convolving this with the Heaviside function. Some description on the derivation is given previously [27]. The deduced relations for each of the Cartesian and curvilinear cases are given below. For an anisotropic case where \(D_{Cx} = 0.3\mu m^2/\text{ms}\) and \(D_{Cy} = D_{Cz} = 0.15\mu m^2/\text{ms}\) the following is obtained for the molar flux, \(\sigma\), that contains the source strength

\[
\sigma = \frac{7.74596669 \left(1 - \text{erf}\left(0.05270462768 \sqrt{30(\Delta x^2 + 2(\Delta y^2 + \Delta z^2))}\right)\right)}{\sqrt{30(x^2 + 2(y^2 + z^2))E_1(0.083333333333\Delta x^2 + 0.1666666667\Delta y^2)}}
\]

A.1
where $E_1(x) = \int_{x}^{\infty} \frac{e^{-t}}{t} \, dt$ is an exponential integral. $\Delta x, \Delta y$ and $\Delta z$ are distances between points in the $x, y$ and $z$ directions, respectively. In the case of the Cartesian coordinates, the molar flux is a scalar. However, in curvilinear coordinates, it is spatially dependent and becomes a vector.

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