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An in vitro-in vivo taste assessment of bitter drug: Comparative electronic tongues study

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Abstract:	<p>Objectives The efficiency of the Astree e-tongue and Taste Sensing system TS5000Z for the evaluation of the taste masking effect of hot melt extruded formulations was investigated in this study.</p> <p>Methods Hot melt extrusion (HME) processing was optimized using Randcastle single screw extruder (USA) to manufacture extrudates with desirable characteristics. Cationic model drug propranolol HCl (PRP) was processed with the anionic polymers - Eudragit L100® (L100) and Eudragit L100-55 (Acryl-EZE). In vitro taste masking efficiency of the two polymers was performed by using two different e-tongues (Astree e-tongue and TS5000Z).</p> <p>Key Findings Both e-tongues were able to detect the taste masking variations of the extrudates and were in good agreement with the in vivo results obtained from a panel of six healthy human volunteers ($R^2 > 0.84$). However, each e-tongue sensor demonstrated different sensitivity suggesting a careful consideration of the experimental findings during melt extrusion is necessary for the development of taste masked formulations. Furthermore, FT-IR spectroscopy and NMR studies revealed possible drug polymer intermolecular interactions as the mechanism of successful taste masking.</p> <p>Conclusions HME can effectively be used to manufacture taste masked extruded formulations while both e-tongues demonstrated satisfactory taste analysis for the development of taste masked formulations.</p>

An *in vitro-in vivo* taste assessment of bitter drug: Comparative electronic tongues study

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1 Abstract

2
3 **Objectives** The efficiency of the Astree e-tongue and Taste Sensing system TS5000Z for the
4 evaluation of the taste masking effect of hot melt extruded formulations was investigated in
5 this study.

6 **Methods** Hot melt extrusion (HME) processing was optimized using Randcastle single screw
7 extruder (USA) to manufacture extrudates with desirable characteristics. Cationic model drug
8 propranolol HCl (PRP) was processed with the anionic polymers - Eudragit L100® (L100)
9 and Eudragit L100-55 (Acryl-EZE). Solid state of the drug in polymer matrices was
10 evaluated by scanning electron microscopy (SEM), differential scanning calorimetry (DSC),
11 particle size analysis, Fourier Transform Infra-Red (FT-IR) and Nuclear Magnetic Resonance
12 (NMR) analysis. *In vitro* taste masking efficiency of the two polymers was performed by
13 using two different e-tongues (Astree e-tongue and TS5000Z). The results obtained from both
14 e-tongues were further compared and contrast to find out the sensor outputs in all
15 formulations.

16 **Key Findings** Solid state analysis of the extruded formulations revealed the presence of
17 amorphous PRP. Both e-tongues were able to detect the taste masking variations of the
18 extrudates and were in good agreement with the *in vivo* results obtained from a panel of six
19 healthy human volunteers ($R^2 > 0.84$). However, each e-tongue sensor demonstrated different
20 sensitivity suggesting a careful consideration of the experimental findings during melt
21 extrusion is necessary for the development of taste masked formulations. Furthermore, FT-IR
22 spectroscopy and NMR studies revealed possible drug polymer intermolecular interactions as
23 the mechanism of successful taste masking.

24 **Conclusions** HME can effectively be used to manufacture taste masked extruded
25 formulations while both e-tongues demonstrated satisfactory taste analysis for the
26 development of taste masked formulations.

27 **Keywords:** Taste masking, Propranolol HCl®, Eudragit L100®, Acryl-EZE, Astree E-
28 Tongue, TS5000Z.

29

30 Introduction

31 Masking the bitter taste of active pharmaceutical ingredients (APIs) is considered a major
32 challenge especially for the development of orally administered dosage forms in
33 pharmaceutical industry. ^[1, 2] Due to the unpleasant sensation bitter taste is always the least
34 desired and sometimes completely undesired option whereas sweet taste is pleasant for most
35 of the people regardless their age and origin. ^[3] In reality most of the APIs used in oral drug
36 products have a bitter taste which is not only undesirable but also frequently has a negative
37 influence on the palatability of the final dosage forms. For paediatric population
38 unpalatable/bitter taste is the most challenging as children are highly sensitive to taste and
39 actively refuse the unpalatable drugs. ^[4, 5] It is often impossible to block bitter taste receptors
40 (due to their increased numbers) from the drug without compromising the mechanism of its
41 action. ^[6, 7] The extent of taste masking of an API depends almost exclusively on the type of
42 formulation (solid or liquid). Being the first preference, commercial oral liquid dosage forms
43 contain artificial sweeteners (e.g saccharin and aspartame) and flavours to mask the tastes
44 which are often limited due to the regulatory requirements. Due to very poor effects of this
45 method and possibilities of toxic and allergic reactions, European Medicines Agency (EMA)
46 strongly recommends another way for taste masking instead of adding sweeteners or flavours.
47 ^[8] An ideal solution for this problem should involve the prevention of any contact of the
48 unpalatable APIs with the taste buds without the addition of taste additives. Such an ideal
49 formulation can be developed by applying an appropriate coating or encapsulation on the API
50 or via manufacturing solid dispersions ^[9, 10] in inert matrices (polymeric/ lipidic). The coated/
51 encapsulated drug then can be dispersed in water.

52 *In vivo* taste masking evaluation studies are performed by healthy human volunteers
53 and involve taste assessments based on the individual scores. ^[11] A well-established statistical
54 method is required to overcome errors and variability between volunteers within the limit of
55 threshold taste perceptions. According to the FDA guidelines studies on paediatric
56 formulations should not be performed on paediatric volunteers due to ethical conflicts. On the
57 other hand in order to design paediatric formulations mature volunteers should also be
58 prohibited due to large physiological differences of taste sensation. ^[7] Ethical doubts on
59 experiments in children and difficulties with interpretation of the results eventually indicate
60 the need to use alternative *in vitro* methods for taste evaluations. ^[4, 7] In the last few years,
61 electronic tongues (e-tongues) became popular for the evaluation of the *in vitro* taste
62 performance for repeatable analysis of pharmaceutical products. ^[12, 13] Electronic tongues are
63 sensor array systems which are able to determine single substances as well as complex
64 mixtures of various substances. Electronic -tongue is a device simulating human sense of

65 taste that allows for the identification and classification of liquid samples. Regardless of the
66 selected chemical compounds e-tongues work to the recognition of general sample properties
67 such as specific taste (e.g bitter). They consist of an array of chemical sensors and a pattern
68 recognition system. [14-16] Over the last few years electronic tongue systems have taken the
69 advantage of different measuring principles including potentiometry, voltammetry and
70 amperometry. Currently, there are commercially available e-tongues which have successfully
71 been employed for taste assessments in various pharmaceutical formulations. Astree e-tongue
72 (Alpha MOS, France) and taste sensing system TS-5000Z (INSENT, Japan) are two common
73 e-tongues which have been used as *in vitro* taste assessment tools [17-21]

74 The aim of this novel study is the evaluations of the taste masking efficiency of hot
75 melt extruded formulations of bitter API (PRP) by using two different e-tongues (Astree e-
76 tongue and TS-5000Z) simultaneously and studying the mechanism of the effective taste
77 masking via extrusion processing.

78 **Materials and methods**

79 **Materials**

80 Propranolol HCl (PRP) was purchased from Sigma Aldrich (London, UK). Eudragit L100
81 (L100) and Eudragit L100-55 (Acryl-EZE) was kindly donated by Evonik Pharma Polymers
82 (Darmstadt, Germany) and Colorcon Ltd respectively. The HPLC solvents were of analytical
83 grade and purchased from Fisher Chemicals (UK). All materials were used as received.

84 **Preparation of formulation blends and hot-melt extrusion (HME) processing**

85 PRP formulations with L100 and Acryl-EZE to be extruded were mixed properly in 100g
86 batches for 10 min each. A Turbula (TF2, Basel) mixer was used to blend the powder
87 formulations (drug/polymers ratio used were 10:90 w/w). Extrusion of all PRP formulations
88 were performed using a Randcastle single-screw extruder (RCP 0625, USA) equipped with a
89 5 mm rod die using 100°C/113°C/155°C/155°C/155°C (Feeder to die) temperature profiles.
90 The screw speed maintained for all extrusion was 15rpm. The produced extrudates (strands)
91 was grinded by using a Ball Milling system (8 balls, 1.5 cm diameter) to obtain granules
92 (<500 µm). Grinding by ball milling was carried out with a rotational speed of 400 rpm for 5
93 min.

94 **Particle morphology and size distribution**

95 Scanning Electron Microscopy (SEM) was used to study the surface morphology of the
96 extrudates. Samples were mounted on an aluminum stage using adhesive carbon tape which
97 was then placed in a low humidity chamber prior to the analysis. Samples were also coated

98 with gold–palladium, and microscopy was performed using Cambridge Instruments - S630
99 (Cambridge, UK) operating at an accelerating voltage of 5 kV. All samples were run singlet.

100 The particle size distribution of the micronized granules of all formulations was
101 measured by dry sieving. The method involved stacking of the sieves on top of each other
102 and then placing the test powder (50 g) on the top sieve. The nest of sieves was subjected to a
103 standardized period of agitation (20 min) and then the weight of the material retained on each
104 sieve was accurately determined to give the weigh percentage of powder in each sieve size
105 range. All samples were run triplicate.

106 **Differential scanning calorimetry (DSC) and Modulated temperature DSC analysis**

107 DSC runs of pure actives, physical mixtures and extrudates were carried out using a Mettler-
108 Toledo 823e (Greifensee, Switzerland) differential scanning calorimeter. Sealed aluminium
109 pans were used to prepared sample weighing about 2-5 mg of samples (n= 3). Samples were
110 heated at 10°C/min heating rate from -40 to 220°C. At the time of heating, samples were
111 under nitrogen atmosphere. In addition modulated temperature differential scanning
112 calorimetry (MTDSC) studies were performed from 25°C to 250°C with an underlying
113 heating rate of 1°C/min. The pulse height was adjusted to 1-2°C with a temperature pulse
114 width of 15-30 s.

115 ***In vivo* taste masking evaluation**

116 *In vivo* taste masking evaluation of pure API, polymers and all active extruded formulations
117 was performed in accordance to the Code of Ethics of the World Medical Association
118 (Declaration of Helsinki).^[19] Six (6) healthy volunteers of either sex (age 18–25) were
119 selected (Male = 3, female = 3) from whom informed consent was first obtained (approved
120 by the Ethics Committee of the University of Greenwich, Ref: UG09/10.5.5.12). All
121 volunteers were also trained prior to the experiment. The equivalent of 100 mg of pure PRP
122 or PRP based extrudates (containing equal amounts of API) were held in the mouth for 60
123 seconds and then spat out. The selection of samples was random and in between of two
124 samples analysis mineral water was used to wash each volunteer's mouth. The bitterness was
125 recorded immediately according to the bitterness intensity scale from 1 to 5 where 1, 2, 3, 4
126 and 5 indicate none, threshold, moderate, bitter and strong bitterness. All samples were
127 evaluated in triplicate.

128 ***In vitro* taste masking evaluation: Astree E-Tongue (Alpha MOS)**

129 The assays were better performed on Astree e-tongue system equipped with an Alpha M.O.S.
130 sensor set #2 (for pharmaceutical analysis) composed of 7 specific sensors (ZZ, AB, BA, BB,
131 CA, DA, JE) on a 48-positions autosampler using 25 ml beakers. Acquisition times were

132 fixed at 120s. ^[19] All the data generated on Astree system were treated using
133 multidimensional statistics on AlphaSoft V12.3 software. Each solution was tested on Astree
134 e-tongue at least 3 times. 3 replicates were taken into account for the statistical treatment. The
135 average values of all sensors signals between 100 and 120 s constitute the raw data for later
136 multivariate statistical data processing. This processing allows to map the data on 2-
137 dimension maps (Principal Components Analysis - PCA, Discriminant Factorial Analysis,
138 Statistical Quality Control, Partial Least Square, etc). With Astree e-tongue, PCA was used
139 to evaluate the differences and similarities between various samples or groups of samples.
140 The samples are represented in a two-dimensional or three-dimensional space with reference
141 to the selected components (PC1 and PCn). The components are classified according to the
142 level of information they produce. Astree sensors were cleaned up with deionised water
143 between each sample measurement.

144 **Sample preparation for Astree E-Tongue**

145 *In vitro* taste masking evaluation was carried out with an Astree E-Tongue equipped with 7
146 different sensor sets. To be as close as panellists taste's conditions, each drug was diluted for
147 60s under magnetic stirring in 25 ml of deionised water to reach API concentration
148 corresponding to a final dose of 100 mg. Then solutions were filtered (as the particles can
149 damage the ASTREE sensors and thus alter the quality of results) with Buchner funnel fitted
150 with filter paper at 2.5µm pore size (Table 1). Analysis for each API was done in triplicate.

151 ***In vitro* taste masking evaluation: TS-5000Z sensing system**

152 The assays were realized on TS-5000Z taste sensing system equipped with a BASIC sensor
153 set (for pharmaceutical analysis) which are suitable for basic APIs composed of 10 specific
154 sensors (AAE, CT0, CA0, C00, AE1, AC0, AN0, BT0, GL1) on a 48-positions autosampler
155 using 25 ml beakers. Each measurement cycle was consisted of measuring a reference
156 solution (Vr) followed by sample solution (Vs) and then the aftertaste (Vr) followed by a
157 cleaning procedure. The "aftertaste" was measured by determining the change in membrane
158 potential caused by the adsorption of the analyte to the lipid membrane. Sensor outputs for
159 both taste (also called relative value (R)) and "aftertaste" were then calculated in relation to
160 the initially determined sensor response to the reference solution (Vr). ^[1, 22] Acquisition times
161 were fixed at 120s with a BT0 negatively charged sensor. All the data generated on TS-
162 5000Z system were treated using multidimensional statistics. Each solution was tested on TS-
163 5000Z at least 4 times and triplicates were taken into account for the statistical treatment.
164 Sensors were then cleaned up in references solutions (30 mM KCl + 0.3 mM tartaric acid)
165 between each sample measurement. The samples were dissolved in 50 mL of 10 mM KCl aq.

166 solutions and further diluted to prepare 0.03, 0.1, 0.3, and 1 mM solutions as standards. Then
167 solutions were filtered with Buchner funnel fitted with filter paper at 2.5 μ m pore size (n=3).

168 FTIR spectroscopy

169 FT-IR analysis was performed on the drug, polymer, drug/polymer physical mixtures, and
170 extrudates using Perkin Elmer PE1600 (Massachusetts 02451
171 USA) Fourier Transform Infrared Spectra according to the KBr disc method from 400 – 3600
172 wavelength/cm⁻¹ range (n=3).

173 Nuclear magnetic resonance (NMR) studies

174 NMR spectra were recorded on a Jeol ECA 500 NMR spectrometer, incorporating a 5mm
175 inverse probe (The ¹H operating frequency was 500 MHz). ¹H NMR spectra of the drugs,
176 polymers and drug/polymer formulations were recorded using the standard Jeol pulse
177 sequence. All samples were dissolved in CD₃OD, degassed and then maintained at 25°C
178 during data acquisition. Samples were referenced with respect to the solvent. The solution
179 concentration of the drug was 2mg/ml, the polymers were 18 mg/ml, and the drug/polymer
180 formulation was 20mg/ml (the overall drug content in the formulations was 10%) (n=3). ¹H
181 T₁ relaxation experiments were recorded for all samples using a standard inverse recovery
182 experiment. Recovery delays (τ) were investigated between 10 ms and 20 s. The relaxation
183 delay was set to be >5T₁. T₁s were calculated from curve fitting and peak intensities which
184 were obtained from the spectra recorded for different recovery delays. Jeol, curve fitting
185 software was utilized during this process.

186 Statistical analysis

187 All data generated and collected during *in vitro* taste analysis by both the e-tongue and taste
188 sensing system TS-5000Z were treated by statistical methods. Results were expressed as raw
189 data in mV of the sample relative measurement to the reference. Sensor signal results were
190 evaluated via multivariate data analysis. Multivariate analysis, such as principal component
191 analysis (PCA), was used to reduce the multidimensional space without losing information.
192 Using PCA, the most abundant information contained in the original data could be
193 transformed into the first principal component (PC-1), and the second most abundant
194 information is transformed into the second component (PC-2). For multivariate data analysis,
195 raw data were pretreated by mean centring and scaling to unit variance. Data processing,
196 graphical illustration and statistical interpretation of the results were carried out using Excel
197 2010 (Microsoft, Redmond, WA, USA). INSENT and Alpha MOS software.

198

199

200 Results and discussion

201 Hot-melt extrusion process: Particle morphology and size distribution

202 Extrusion processing of all PRP based formulations was performed at 155°C with relatively
203 lower screw speed of 15 rpm in order to allow homogenous blending of the drug/polymer
204 binary mixtures. The rationale underlying selecting high processing temperature was due to
205 the higher Tgs of polymeric carriers used. Various formulation trials were conducted at the
206 optimization stage ranging a drug loading 10-20% (w/w ratios). But keeping the final dose in
207 the finished product e.g. tablets in account, 10% (w/w) drug loading was chosen to proceed
208 with. Preliminary results showed no significant differences in terms of the solid state of the
209 extrudates and physical performance between the formulation containing 20% PRP and 10%
210 PRP. Another reason underlying the selection of PRP- a cationic charged substance, as a
211 model drug and two different polymers (anionic charged) as carriers, was to possibly
212 facilitate an intermolecular interactions in order to mask unpleasant taste of the bitter API.
213 Theoretical miscibility parameter calculations showed that the solubility parameter of PRP
214 (21.94 MPa^{1/2}) calculated by Van Krevelen equation is quite close to that of L100 (22.75
215 MPa^{1/2}) and Acryl-EZE (21.65 MPa^{1/2}).^[6] It has been reported in previous studies that if the
216 difference of the solubility parameters between drug and polymer is less than 7MPa^{1/2}, then
217 the polymer is likely to be miscible with the API to form an amorphous solid dispersions.^[6]
218 As a result the cationic PRP may interact with the functional groups of the negatively charged
219 polymers to effectively mask bitter taste of the drug.

220 SEM was used to examine the surface morphology of the drug and extrudates. The
221 extrudates containing L100 and Acryl-EZE showed homogenous particles distribution on the
222 extrudates surface with PRP (Fig. 1) indicating excellent HME processing of the extruded
223 materials to form solid dispersions. The particle size distribution depicted in Fig. 1 shows
224 particle sizes lower than 500 µm for most formulations ranging from 40 – 400µm. A small
225 percentage can be seen at sizes <40µm as the milling process was optimized to reduce fines
226 in the final extruded batches.

227 Solid state analysis

228 DSC was conducted in order to analyze the solid state (crystalline or amorphous) of the pure
229 drug, polymers, drug/polymers binary mixtures and drug/polymer extrudates. The thermal
230 transition of PRP in Fig. 2 showed an endothermic peak corresponding to its melting point at
231 166.65°C ($\Delta H = -126.25$ J/g). The bulk polymers showed Tgs at 83.97°C and 164.83°C
232 corresponding to Acryl-EZE and L100, respectively (Fig. 2). A sharp melting peak was also
233 observed in the Acryl-EZE thermogram at 59.2°C (data not shown), corresponds to the

234 presence of crystalline plasticizers in the co-processed formulation.^[19] MTDSC analysis of
235 the binary physical blends of PRP/L100 and PRP/Acryl-EZE exhibited PRP endothermic
236 peaks shifted at slightly lower temperatures of 162.41°C to 153.62°C indicating a
237 drug/polymer interaction at small extent. The same shift at lower temperatures was also
238 observed for the Tgs of the polymers at 73.16°C and 98.82 °C for PRP/Acryl- EZE and
239 PRP/L100, respectively.

240 Furthermore, the extruded PRP/Acryl-EZE (and L100) extrudates exhibited single
241 glass transition peaks at 63.36 and 74.84°C, respectively which indicates the presence of
242 drug/polymers miscibility and formation of molecular solid dispersions. When the two
243 components are miscible the Tg of the extruded sample lies between the Tgs of the individual
244 components (amorphous drug and polymers) according to Gordon – Taylor equation. [6, 19]
245 The Tg of PRP was determined at 34.74°C (data not shown). DSC analysis confirmed the
246 presence of molecular dispersions in all extruded formulations.

247 Previous studies^[6] showed that the diffraction patterns of both PRP physical mixtures
248 exhibited crystalline peaks with reduced intensities corresponding to pure drug. The
249 diffractograms of the extruded formulations were characterized with the absence of drug
250 intensity peaks indicating amorphous or molecularly dispersed state.

251 ***In vivo* taste masking**

252 The masking efficiency of the developed granules was evaluated *in vivo* (approved by
253 University of Greenwich, UK ethics committee) with the assistance of six healthy human
254 volunteers (age 18 – 25). The statistical data collected from the *in vivo* study for the pure
255 active substance and the extruded formulations are depicted in Fig. 1. The data analysis
256 showed significant suppression ($p < 0.05$) of the bitter taste for the API. These results
257 demonstrate the influence of the polymeric carriers and importance of drug loading in the
258 final formulation. Both polymers showed effective taste masking capacity with descending
259 order L100 > Acryl-EZE. Furthermore, the HME formulations presented excellent masking
260 effect for active concentrations (10%) of the API. This could be due to the possible drug
261 polymer interactions in the solid dispersions manufactured during extrusion process. In the
262 solid dispersions cationic active substance (PRP) may have interacted with the functional
263 group of the negatively charged polymers. These interactions facilitated a hydrogen bonding
264 interaction between the active amide group of API and carboxylic group of polymers and
265 consequently masked the bitter taste of the active. A similar study has also been reported
266 elsewhere.^[2] In Fig. 3 the sensory data obtained from the panelists interestingly showed that
267 the taste masking efficiency of L100 is not similar to that of Acryl-EZE for the API used.
268 This could be attributed to the pH dependant dissolution properties of Acryl-EZE ($\text{pH} \geq 5.5$)

269 compared to that of L100 ($\text{pH} \geq 6$) as the saliva represents a basic pH (~ 7.4) in healthy
270 individuals. However, the sensory scores of the API in different formulations are within the
271 range (below 2) which has been demonstrated as optimum by *in vitro* evaluations. [1, 11]

272 *In vitro* taste evaluations (Astree e-tongue)

273 Astree e-tongue was used for *in vitro* taste analysis of the drug and active formulations.
274 Principal Component Analysis (PCA) associated to complementary data processing was used.
275 [20] Based on the statistical analysis taste maps were constructed in order to determine the
276 distances between active and polymer solutions. Actually the distance between each active
277 formulation and its corresponding placebo is indicative of how close or how far the taste of
278 the two samples is. The interpretation of the taste maps suggests that the shorter the distance
279 (Euclidean distance) between active and placebo (polymer), the better the taste masking of
280 the active ingredient. Thus the distance between any drug polymer pairs in the taste maps is
281 indicative of the taste masking efficiency of the extruded polymer formulations from which
282 the estimated Discrimination Index (DI in %) can be determined for each solution. This
283 indicator (DI) takes into account the average difference between the pairs (i.e drug and active
284 formulation or polymer and active formulation) to compare the dispersion or taste masking
285 effect. It is assumed that the higher the DI values (maximum 100%), the longer the distance
286 between groups and the lower the masking effects.

287 In Fig. 4a, the taste map shows significant discrimination between placebo and active
288 solutions with PRP. Liquid sensors were able to detect the presence of the drug in the
289 extruded formulations. Considering the pure drug in deionized water the extrudates with
290 L100 (10% drug loading w/w) shows a better taste improvement compared to that of Acryl-
291 EZE (Fig. 4a). The distance between the placebo and the active formulations indicates the
292 efficiency of the taste masking of the active by both polymers. The observed distance
293 proximity between extrudates of PRP and placebo is noticeable (for an example, 19% taste
294 improvements of PRP with L100). This trend is likely to be linked with a pH influence of
295 Acryl-EZE in deionized water ($\text{pH} \sim 5.5$) which leads to a higher separation of placebo from
296 the active formulations by dissolving faster than L100 ($\text{pH} > 6.0$). From the PCA graphs it
297 can be seen that the placebo, the API, and the extrudates are discriminated which means
298 significant taste differences.

299 Based on the Astree e-tongue experimental results it was also possible to design the
300 DI graphs for the drug – polymer combinations. In Fig. 4b, it can be seen that the distance
301 between active and placebo formulations with Acryl-EZE (DI 62%) is higher than that of

302 L100 (DI 40%) in the extrudates, indicating better taste masking efficiencies of L100 (19%
303 taste masking/improvement) than Acryl-EZE polymeric system.

304 However, this was expected as the use of deionized water was intentionally selected
305 in order to test the sensitivity of the Astree e-tongue in variations of the drug dissolution
306 rates. As mentioned above the polymers dissolve in different pH which results faster drug
307 release for Acryl-EZE compared to L100.

308 Sensory correlated models based on Partial Least Square (PLS) were built to evaluate
309 the correlation with sensory scores. The correlation model is considered as valid and fits with
310 panel perception ($R^2 > 0.80$). But it should be taken with care as all data on sensory tests
311 (number of panelists, variability on measurement) were not communicated. It's quite obvious
312 from the Fig. 4c that the *in vitro* taste assessment studies carried out with Astree e-tongue
313 correlated very well with the *in vivo* panelists data ($R^2 = 0.9892$ (Acryl-EZE); 0.9959
314 (L100)).

315 PRP was found to be quite bitter by the panelists (sensory score 5) similar to the
316 Astree e-tongue evaluation. The impact of Acryl-EZE carrier was negligible as Acryl-EZE
317 itself was also found not to be bitter (sensory score 1). **Contrary**, PRP/L100 formulations
318 demonstrated improved taste masking even though the bulk polymer showed threshold-
319 moderate bitterness. However, the PLS were in good agreement by complementing the *in*
320 *vivo* study, where the panelists recorded a moderate taste with L100 (and no taste with Acryl-
321 EZE).

322 A further statistical analysis was performed by considering the standard deviations
323 (SD) and therefore the relative standard deviations (RSD) of all extruded formulations. The
324 findings of the standard deviations studies for bulk drugs and the extrudates are summarized
325 in Table 2. It can be seen that the statistical analysis of SD and RSD for all formulations,
326 showed positive results towards effective taste masking of bitter PRP. It is accepted that the
327 scale of interpretation measure is $SD < 50$: Fair and $SD < 30$: good, respectively. Based on
328 this scale of interpretation, the results showed (Table 2) that the calculated mean SD values
329 for all formulations is ≤ 13 which suggests good taste masking of the API in the extruded
330 formulations.

331

332 **INSENT TS-5000Z sensing system**

333 The *in vitro* masking effect of the extruded formulations in artificial saliva was also evaluated
334 by using the INSENT TS-5000Z e-tongue. The distance percentages (%) between active
335 substances and formulation solutions were estimated in four different time intervals (0.5 min,

336 1 min, 10 min and 30 min) as they are indicative of taste masking efficiency of the extruded
337 formulations. In addition, the discrimination index (DI, %) was determined for each solution.
338 Initial trials showed that the BT0 sensor of TS-5000Z system responded to the DPD and PRP
339 at the each concentration ranging from 0.03, 0.1, 0.3 and 1 mM. Therefore, BT0 sensor can
340 be useful for detecting bitterness of the API in the concentration ranging from 0.03 to 1 mM.

341 In contrast with the Astree e-tongue, in INSENT TS-5000Z system, the lower DI
342 values the longer the distance in taste responses between the pairs (drug and formulations)
343 and thus a higher discrimination, which means greater masking effect. The DI (%) values can
344 help to assess the significance of difference between the formulations. In Fig. 5a the bitter
345 taste suppression of PRP in the L100 extrudates is quite significant even after 30 min as the
346 DI index (%) is only about 60% while after 1 min DI is 40% (DI index (%) close to 0%
347 indicates no taste). In contrast the PRP/ Acryl-EZE extrudates (Fig. 5b) did not show taste
348 suppression similar to the L100 polymer but still the DI index (%) estimated by the BT0
349 sensor around 98% after 30 min and 85% in 1 min, respectively was considered effective (but
350 less than L100).

351 The normalized taste graphs showed significant discrimination between all active
352 formulations and active ingredient solutions (Fig. 5a-b) suggesting lower taste masking
353 efficiency of Acryl-EZE for the API compared to the taste suppression of L100.

354 As mentioned before, liquid sensors are able to detect the taste of the drug in the
355 masked formulations (up to 0.3mM API), therefore the *in vitro* taste masking results detected
356 by the BT0 sensor are quite sensitive and consistent. For that reason, in comparison with the
357 pure drug in the reference solutions (artificial saliva) the extrudates exhibited taste masking
358 effects. As mentioned above this could be attributed to the pH dependency of both polymers
359 which present different drug release due to their different pH values. However the e-tongue
360 sensor did perceive the taste of bitter APIs from the dissolved polymer matrices.

361 Sensory correlated models were built to evaluate the correlation with sensory scores.
362 The correlation model was considered as valid and fitted with panel perception (Fig 5c) and
363 complemented the sensory findings from the panelists' scores to conclude the statement that
364 L100 has better taste masking efficiency than Acryl-EZE. The TS-5000Z taste sensing
365 system demonstrated different sensitivity to each sample with high correlation ($R^2=0.94$) to
366 the taste scores, suggesting that the sensor responds selectively according to bitterness
367 intensity by providing quantitative information.

368 The BT0 sensor was also used to determine the taste of pure polymers. Interestingly
369 as shown in Fig. 5d it was not possible to detect any taste for both L100 and Acryl-EZE.

370 Apparently the contribution of the bulk polymers was not taken in account as INSENT uses a
371 different approach compared to that of Astree e-tongue.

372

373 **Fourier Transform Infra-Red (FT-IR) analysis**

374 FT-IR has been used to study interactions in drug/polymer dispersions by providing valuable
375 information regarding the oppositely charged ionic drug/polymer interactions at molecular
376 level. [23] By showing the appearance of additional bands, alterations in wavenumber position
377 or broadening of functional groups compared to the spectra of the pure drug and polymer the
378 FTIR spectra gives an indication of drug/polymer interactions. The FTIR spectra for the
379 extruded formulations are shown in Fig.6.

380 The characteristic bands of CO- vibrations of the carboxylic acid groups in L100 and
381 Acryl-EZE are shown at $\sim 1705\text{ cm}^{-1}$ and of the esterified carboxylic groups at $\sim 1735\text{ cm}^{-1}$.
382 The FTIR spectra of the PRP extrudates in comparison with the pure materials are depicted in
383 Fig. 6, which showed a new absorption band at ~ 1560 and $\sim 1555\text{ cm}^{-1}$ for PRP/ L100 and
384 PRP/ Acryl-EZE, respectively. This is considered to be the result of the presence of amine
385 group alongside the carboxyl group in the solid dispersions. [24] During the FTIR process the
386 resonance is possible between the two CO-bands within COO- groups. As a result, the
387 characteristic CO- absorption is replaced by the band of auto-symmetrical vibrations of the
388 COO- group in the $1555\text{--}1560\text{ cm}^{-1}$ region of the FTIR spectra [24, 25] which belongs to the
389 polymer (L100 or Acryl-EZE). This type of spectra changes provides strong evidence of
390 strong interactions between the anionic methacrylate polymers (-COO) and the cationic PRP
391 (amine group) by enabling the formation of hydrogen bonds with the amine group of the
392 drug.

393 **NMR analysis**

394 ^1H T₁ NMR spectroscopy was employed to monitor the possible chemical changes at the
395 molecular level by analyzing chemical shifts of NMR signals. Such a change has been
396 observed in regards with the chemical shifts in the ^1H NMR spectra of drug and drug/polymer
397 solutions. [26, 27] Previous studies showed that NMR analysis carried in DMSO successfully
398 revealed possible drug/polymer interactions in molecular level. Initially solid state NMR was
399 conducted in order to elucidate possible drug/polymer interactions; however the low drug
400 loading in our formulations didn't accord NMR a meaningful interpretation.

401 ^1H T₁ NMR experiments were used to analyse spin relaxation times. Different
402 relaxation rates of nuclear spins can be related to aspects of molecular structure and
403 additionally to internal molecular motion. The reasoning behind these experiments was to

404 look at potential changes of the drug's molecular motion, before and after the extrusion.
405 Indeed, it would be assumed that the free drug (with a low molecular weight) would have
406 quite a high molecular motion leading to fairly high T_1 relaxation delays. After formulation,
407 any consequence of an interaction between the drug and polymer would result in a decrease
408 in the amount of molecular motion observed for the drug. It can be seen in Fig. 7 that the T_1
409 relaxation times have significantly been decreased in all PRP/L100 formulations. About 16-
410 20 folds of decrease in the T_1 relaxation times have been observed in the extruded
411 formulations. This significantly indicates that the free drug (with a low molecular weight) had
412 quite a high molecular motion leading to fairly high T_1 relaxation delays (times) while the
413 extruded formulations showed very low T_1 relaxation delay. This was due to the strong
414 drug/polymer interactions leading to a significant decrease in the relaxation time. T_1
415 relaxation delays are particularly sensitive to intermediate molecular motions which result in
416 short T_1 s. Molecules which have fast or slow molecular motion can have comparable T_1 s. [6]

417 This NMR analysis indicates the presence of molecular interaction between the drug
418 and polymers in solutions, although the type of the interactions cannot be elucidated. In
419 addition, the presence of such intermolecular interaction can contribute to the possible taste
420 masking mechanism of all drug/polymer combinations during extrusion.

421

422 **Conclusions**

423 In this study the performance of two e-tongues was evaluated for the development of taste
424 masked PRP formulations processed by hot melt extrusion. The optimized formulations were
425 also evaluated *in vivo* by panellists and showed very good masking efficiency. Both e-
426 tongues confirmed that the extruded formulations of PRP/L100 demonstrated better taste
427 masking compared to those of PRP/ Acryl-EZE. However, each e-tongue interpreted different
428 extent of taste masking efficiency. The e-tongues evaluation suggests that results should be
429 cautiously considered in comparison to panellist's scores. The NMR and FT-IR analysis
430 confirmed possible drug/polymer intermolecular interaction which could explain the
431 mechanism underlying the taste suppression in all extruded formulations.

432 **Acknowledgements**

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434 Dr Massaki Habara and Teraoka Makoto (INSENT, Japan) for their support to run the *in vitro*
435 taste assessment studies.

436 **Conflict of interest**

437 The authors report no conflicts of interest.

438 **Abbreviations**

439 Active pharmaceutical ingredient, API; Differential Scanning Calorimetry, DSC; Dispersion
440 Index, DI; Eudragit L100, L100; European Medicines Agency, EMA; Fourier Transform
441 Infra-Red, FT-IR; Food and Drug Administration, FDA; glass transition, T_g; Hot melt
442 extrusion, HME; Nuclear Magnetic Resonance, NMR; propranolol HCl, PRP; Partial Least
443 Square, PLS; Principal Component Analysis, PCA; Relative standard deviation, RSD;
444 Scanning Electron Microcopy, SEM; Standard deviation, SD.

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541 **Tables**

542

543 **Table 1:** Sample preparation for taste masking analysis

Description	Type	Drug (%)	Polymer (%)	Drug (mg)	Polymer (mg)	Total (mg)
PRP	Active	100	0	100	0	100
Acryl-EZE	Polymer	0	90	0	900	900
PRP/ Acryl-EZE	Extrudates	10	90	100	900	1000
L100	Polymer	0	90	0	900	900
PRP/L100	Extrudates	10	90	100	900	1000

544

545

546 **Table 2:** Mean standard deviation (SD) and relative standard deviation (RSD) for each
547 solution for *in vitro* taste analysis by Astree e-tongue.

PRP dissolution after 60s			
Formulation	Mean SD	Mean RSD (%)	Interpretations
PRP	8.0	0.7	Good
PRP/ Acryl-EZE	12.0	0.9	Good
PRP/L100	10.0	1.4	Good
Acryl-EZE	13.0	1.1	Good
L100	8.0	0.8	Good
AVERAGE	13.0	0.7	Good

548
$$RSD = \frac{SD}{\bar{x}} \times 100$$

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561 **Figures Caption List**

562

- Fig. 1** SEM images of PRP/polymer extrudates and particle size distribution.
- Fig. 2** DSC thermal transitions of (i) PRP and polymers pure, (ii) PRP/polymer extruded formulations.
- Fig. 3** Sensory scores of all formulations by panelist (n=6).
- Fig. 4a** Signal comparison between active and placebo formulations with L100 and Acryl-EZE and PRP (dissolution for 60s).
- Fig. 4b** Distance and discrimination comparison between signal of PRP pure and their formulations on Astree e-tongue (after 60s dissolution).
- Fig. 4c** Sensory correlation model based on PLS with Astree e-tongue
- Fig. 5a** Normalised DI (%) of all drug/L100 formulations in four different time scale.
- Fig. 5b** Normalised DI (%) of all drug/ Acryl-EZE formulations in four different time scale.
- Fig. 5c** Relationship between results of taste sensors and human taste scores for similar tastes. The standard deviations on the x- and y-axes are the difference between the panelists' scores and measurement error (n = 6), respectively.
- Fig. 5d** Sensor output of the two polymers, Acryl-EZE and L100. Maximum concentrations of polymers were set at 60 times the maximum API conc. (approx. 0.5 mg/mL x 60 = 30 mg/mL).
- Fig. 6** FT-IR spectra of PRP extruded formulations.
- Fig. 7** Part, ¹H T1 spectra (aromatic region) for the PRP pure and taste masked formulations.

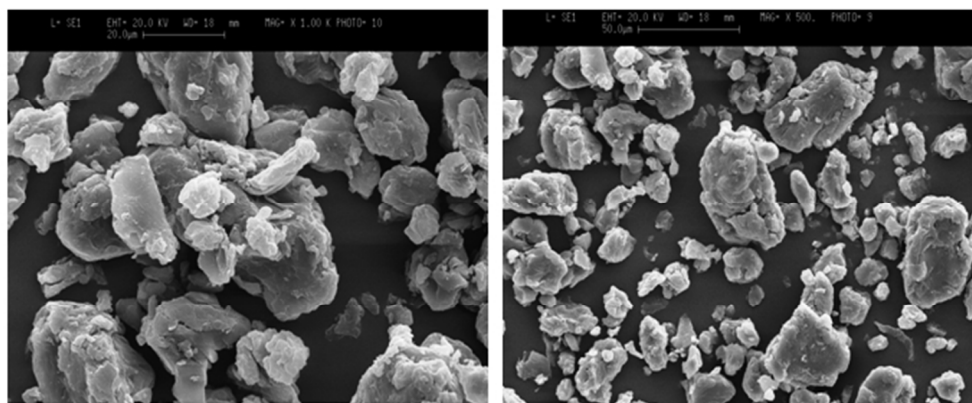
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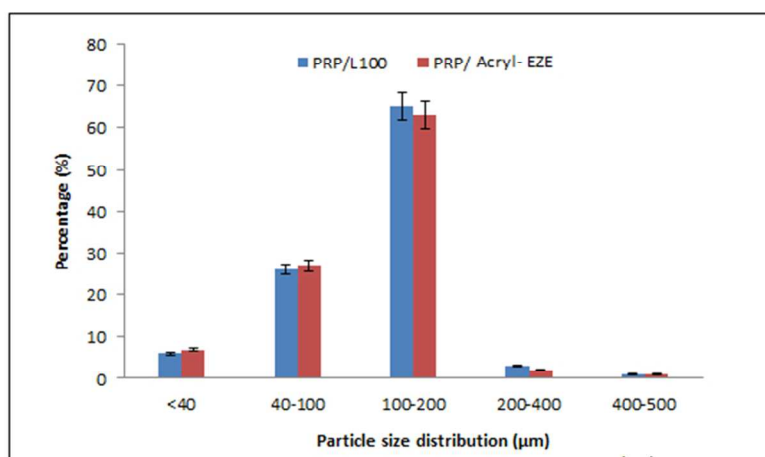
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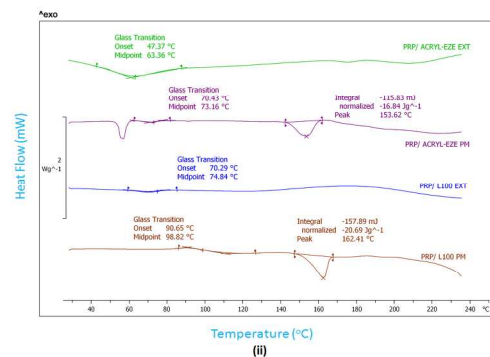
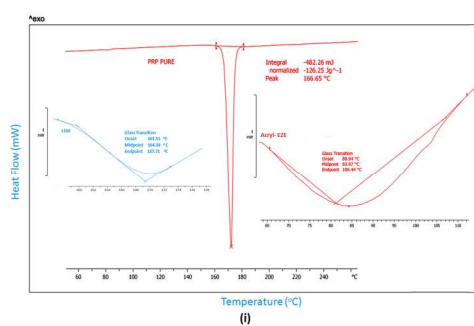
(i) PRP/L100

(ii) PRP/Acryl-EZE



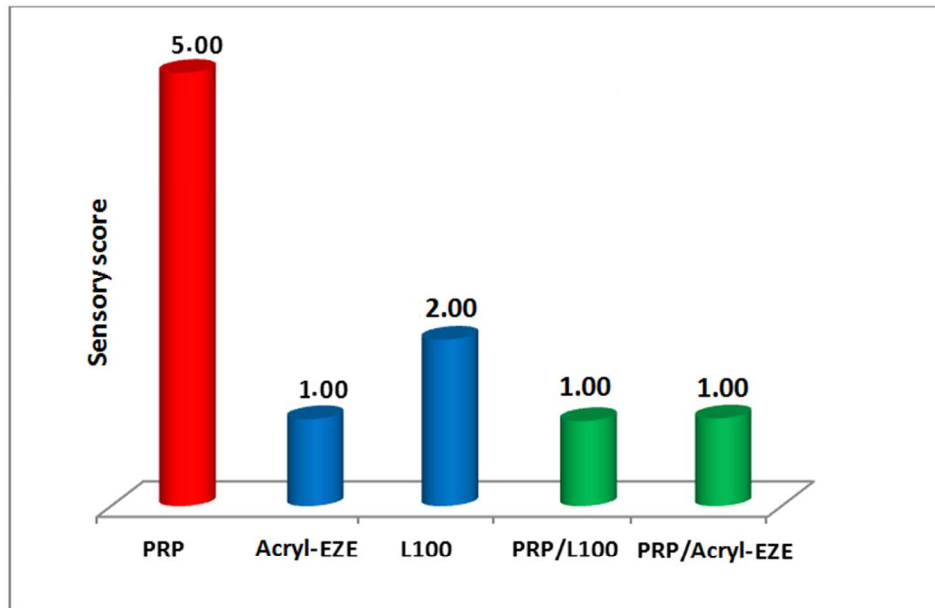
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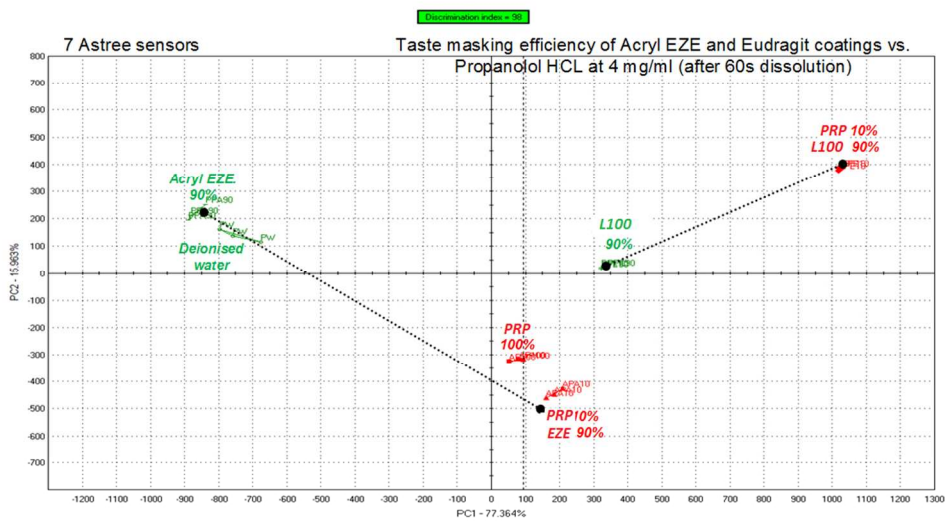
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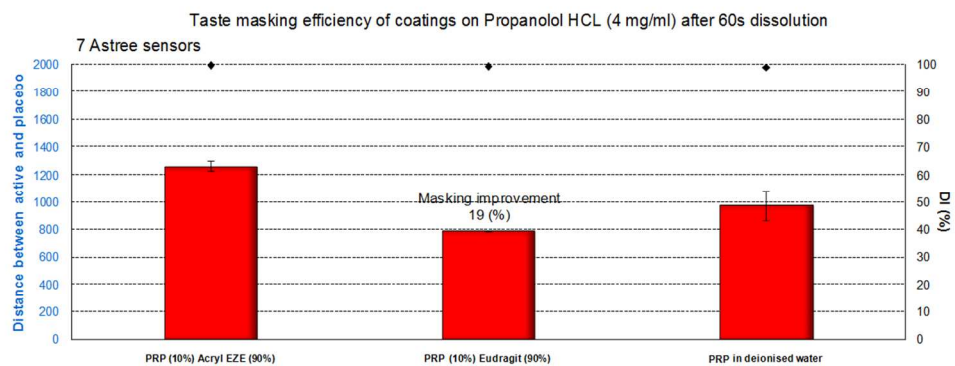
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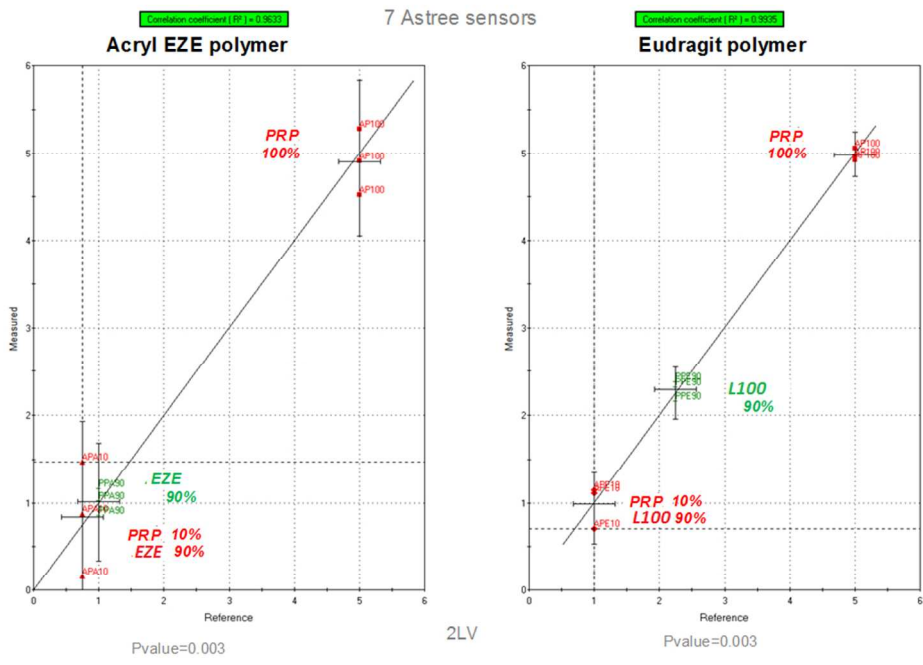
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318x131mm (96 x 96 DPI)

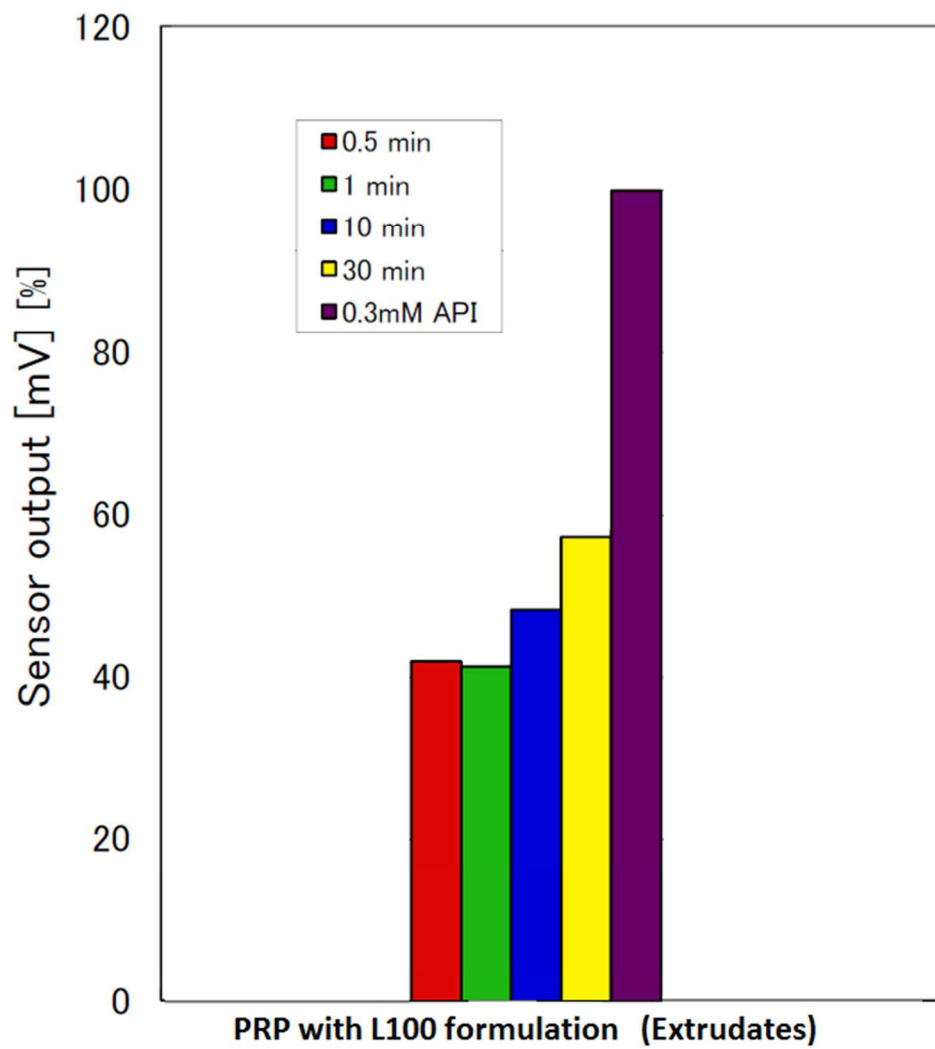
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Taste correlation of polymer's formulation vs. propranolol solution (dose 100 mg)

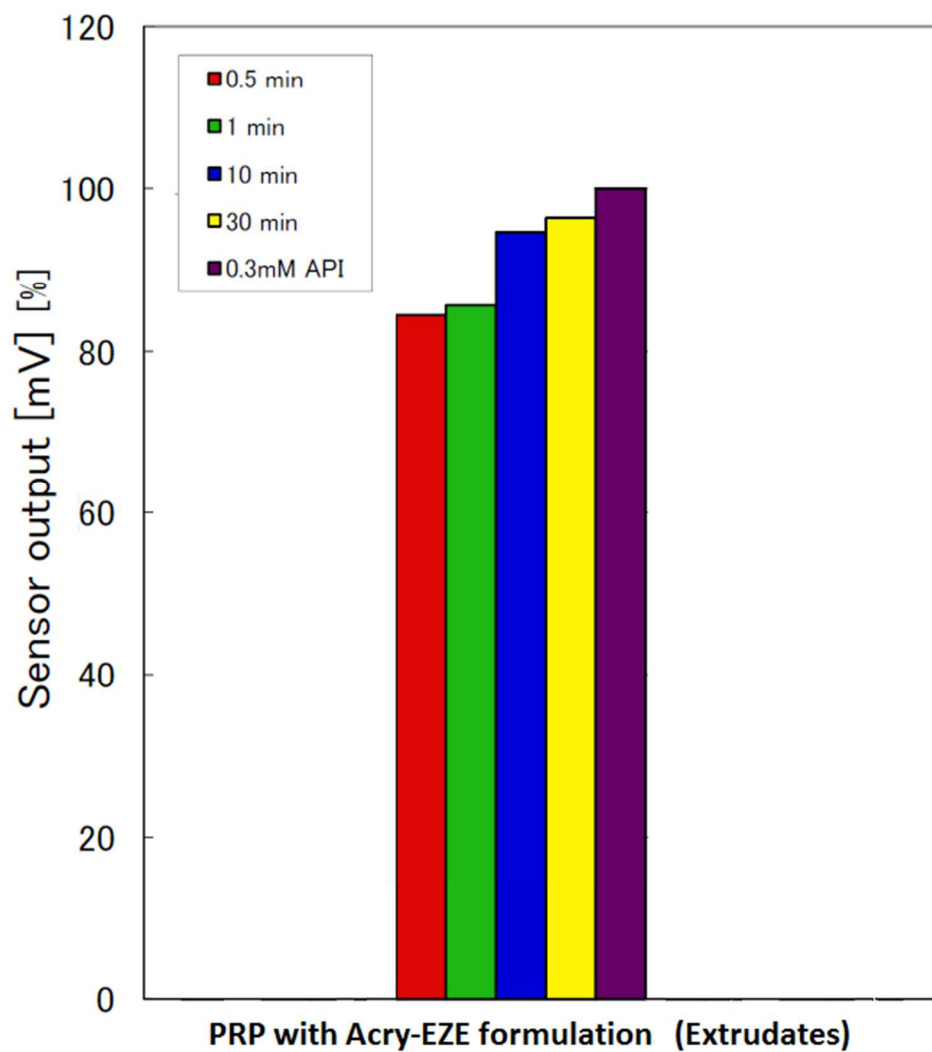


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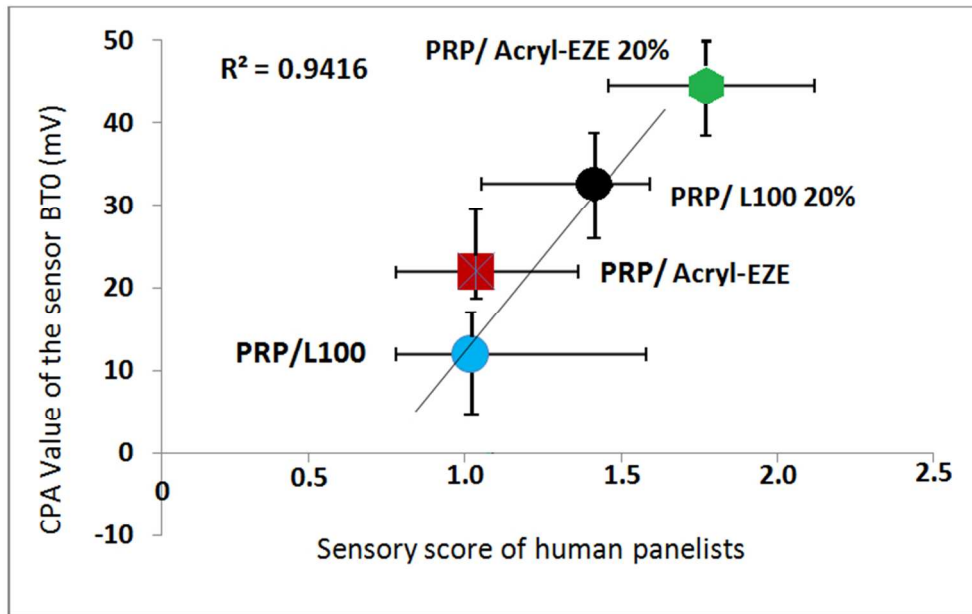
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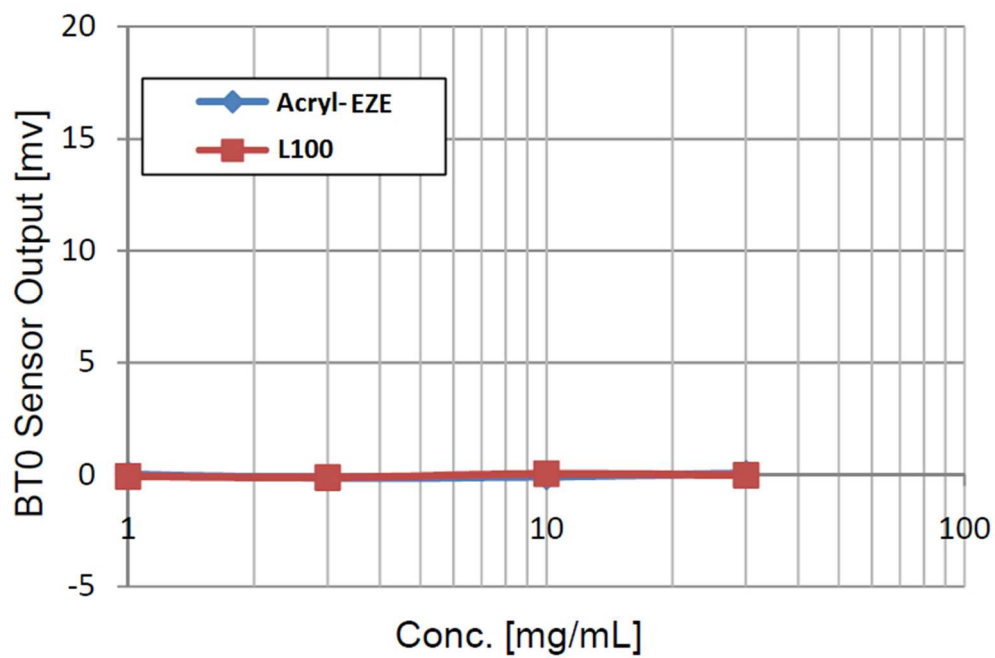


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210x132mm (96 x 96 DPI)

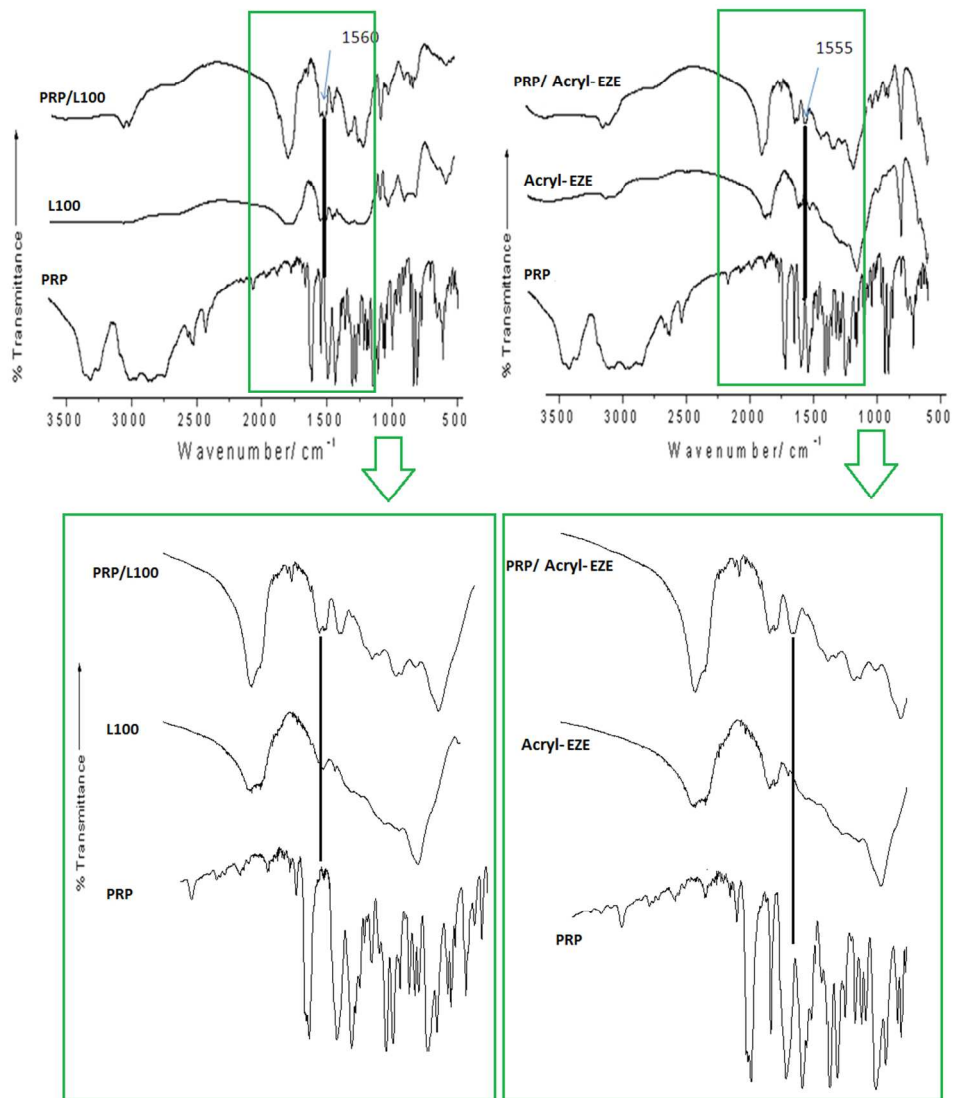
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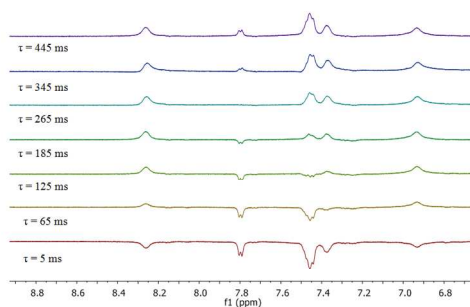
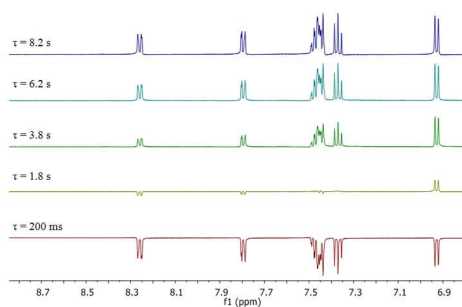
mg/mL	Acryl-EZE (mV)	L100 (mV)
1	0.01	-0.06
3	-0.14	-0.12
10	-0.08	0.05
30	0.07	-0.01

218x203mm (96 x 96 DPI)





308x351mm (96 x 96 DPI)

Part, ^1H T1 spectra (aromatic region) for the PRP/L100Part, ^1H T1 spectra (aromatic region) for the PRP

465x166mm (96 x 96 DPI)

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